



Evolution of real contact area under shear and the value of static friction of soft materials

R. Sahli^a, G. Pallares^{a,b}, C. Ducottet^c, I. E. Ben Ali^d, S. Al Akhrass^d, M. Guibert^a, and J. Scheibert^{a,1}

^aLaboratoire de Tribologie et Dynamique des Systèmes UMR5513, Université de Lyon, Ecole Centrale de Lyon, Ecole Nationale d'Ingénieurs de Saint-Etienne, Ecole Nationale des Travaux Publics de l'Etat, CNRS, F-69134 Ecully, France; ^bLaboratoire d'Innovation Numérique pour les Entreprises et les Apprentissages au service de la Compétitivité des Territoires, Centre des Etudes Supérieures Industrielles, F-34070 Montpellier, France; ^cLaboratoire Hubert Curien UMR5516, Université de Lyon, Université Jean Monnet Saint-Etienne, CNRS, Institut d'Optique Graduate School, F-42023 Saint-Etienne, France; and ^dIngénierie des Matériaux Polymères UMR5223, CNRS, Université Claude Bernard Lyon 1, Université Jean Monnet Saint-Etienne, Université de Lyon, Institut National des Sciences Appliquées Lyon, F-69622 Villeurbanne, France

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The frictional properties of a rough contact interface are controlled by its area of real contact, the dynamical variations of which underlie our modern understanding of the ubiquitous rate-and-state friction law. In particular, the real contact area is proportional to the normal load, slowly increases at rest through aging, and drops at slip inception. Here, through direct measurements on various contacts involving elastomers or human fingertips, we show that the real contact area also decreases under shear, with reductions as large as 30%, starting well before macroscopic sliding. All data are captured by a single reduction law enabling excellent predictions of the static friction force. In elastomers, the area-reduction rate of individual contacts obeys a scaling law valid from micrometer-sized junctions in rough contacts to millimeter-sized smooth sphere/plane contacts. For the class of soft materials used here, our results should motivate first-order improvements of current contact mechanics models and prompt reinterpretation of the rate-and-state parameters.

area of real contact | rough contact | elastomer | static friction | rate-and-state friction

Rough solids in dry contact touch only at their highest asperities, so that real contact consists of a population of individual microjunctions (Fig. 1*B*), with a total area A^R . A^R is usually much smaller than the apparent contact area, A^A , that one would expect for smooth surfaces. Since the seminal work of Bowden and Tabor (1), it is recognized that the frictional properties of such multicontact interfaces are actually controlled by A^R rather than by A^A . In particular, direct measurements of A^R on transparent interfaces have been developed (2, 3) and repeatedly found proportional to the friction force, both for multicontacts (4–10) and for single contacts between smooth bodies (1, 11, 12), with the proportionality constant being the contact's frictional shear strength, σ . A^R is a dynamic quantity with three major causes for variations.

First, A^R is roughly proportional to the normal load applied to multicontacts (5, 6, 10). This result, which provides an explanation for Amontons–Coulomb's law of friction (friction forces are proportional to the normal force), has been reproduced by many models of weakly adhesive rough contacts under purely normal load (1, 4, 13–16). In the case of independent elastic microjunctions, although each of them grows nonlinearly with normal load, proportionality arises statistically due to randomness in the surface asperities' heights (13). Second, in static conditions, A^R slowly increases, typically logarithmically, with the time spent in contact (5, 17). This phenomenon, so-called geometric aging (18), is interpreted as plastic (5, 19, 20) or viscoelastic (21) creep at the microjunctions, depending on the materials in contact, and is different from contact strengthening with time at constant contact area (18, 22), so-called structural aging. Third, at the onset of sliding of the interface, the population of already aged microjunctions gradually slips and is replaced

by new, smaller microjunctions. Slip inception is thus accompanied by a drop of A^R (5, 17), by up to a few tens of percent. This effect is often considered to be the origin of the difference between the peak (static) and steady sliding (kinematic) friction forces (18).

Accounting for these three dependencies together has been a major success in the science of friction because it provides a consistent picture of the physical mechanisms underlying the ubiquitous state-and-rate friction law (5, 18, 20–31), which is obeyed by multicontacts in a variety of materials, from polymer glasses to rocks, through rubber and paper. However, a series of experimental observations reported here and there in the literature over recent decades suggest that the picture may not be fully comprehensive yet. These observations, made on smooth contacts, have repeatedly indicated that the area of apparent contact, A^A , depends on the value of the tangential load, Q , applied to the interface. For instance, smooth metallic sphere/plane contacts typically grow as Q increases (1, 2), due to plastic deformations in the vicinity of the contact (1, 32). Conversely, A^A decreases when smooth elastomer-based sphere/plane contacts as well as fingertip contacts are increasingly sheared (9, 33–38), presumably due to viscoelastic and/or adhesion effects (33, 36, 38–40). It is therefore tempting to hypothesize that not only smooth but also rough interfaces have a dependence of their contact area on the tangential load, Q . Such a dependence would directly affect the resistance to sliding of a rough contact, the way we use current contact and friction models to predict the static friction force, and the physical meaning of the parameters of the rate-and-state friction law. To test this hypothesis, we carried out experiments to monitor, in multicontacts involving elastomers or human fingertips, the evolution of A^R when Q is increased from 0 to macroscopic sliding.

Significance

We investigate the origin of static friction, the threshold force at which a frictional interface starts to slide. For rough contacts involving rubber or human skin, we show that the real contact area, to which static friction is proportional, significantly decreases under increasing shear, well before the onset of sliding. For those soft materials, our results will impact how we use and interpret current contact mechanics and friction models.

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¹To whom correspondence should be addressed. Email: julien.scheibert@ec-lyon.fr.

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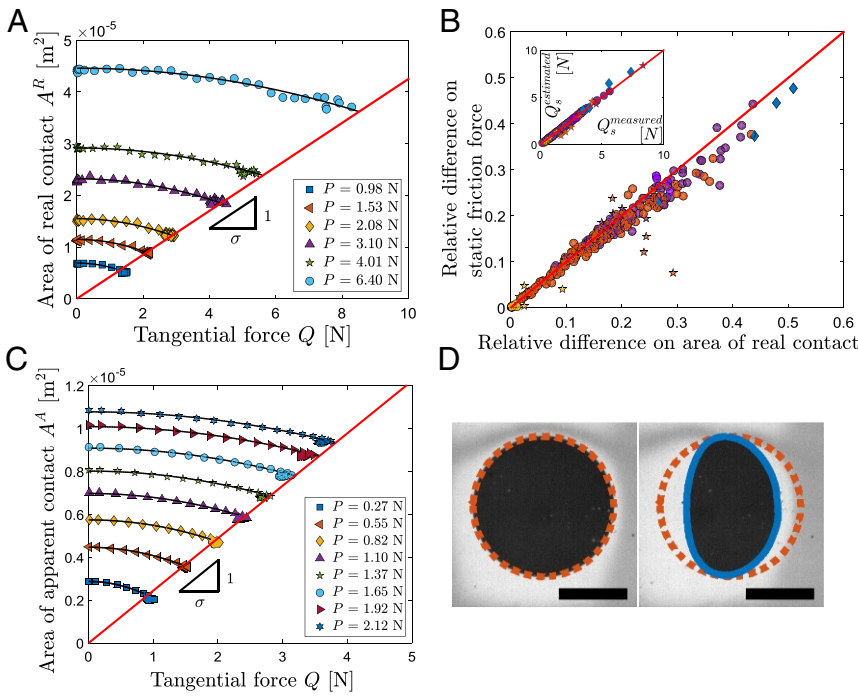


Fig. 2. Area reduction and static friction. (A) A^R vs. Q , for a PDMS/glass multicontact submitted to various normal loads P (1 point of 130 shown). $R_q = 26 \mu\text{m}$. $V = 0.1 \text{ mm/s}$. Solid curves: quadratic fits of the form of Eq. 1. Solid straight line: linear fit through data points corresponding to the onset of macroscopic sliding. See *Materials and Methods* for the value of σ . (B, Inset) Static friction force estimated using Eq. 3, $Q_s^{\text{estimated}}$, vs. its measured value, Q_s^{measured} , for all experiments, including different velocities. (B, main plot) $(\sigma A_0^R - Q_s^{\text{estimated}})/\sigma A_0^R$, as a function of $(A_0^R - A_s^R)/A_0^R$. In both plots, the solid straight line has slope 1 and goes through the origin. Purple, PDMS/glass interfaces; yellow, PDMS/grafted PDMS; orange, PDMS/cross-linked PDMS; stars, multicontacts; circles, smooth sphere/plane contacts; blue diamonds, fingertip/glass contacts. $V = 0.1 \text{ mm/s}$ except light purple circles ($V = 0.05 \text{ mm/s}, 0.1 \text{ mm/s}, 0.5 \text{ mm/s}, 1 \text{ mm/s}$ for PDMS/glass at $P = 1.1 \text{ N}$). (C) A^A vs. Q , for a smooth PDMS/glass sphere/plane contact, presented as in A. One point of 70 is shown. $R = 9.42 \text{ mm}$. $V = 0.1 \text{ mm/s}$. See *Materials and Methods* for the value of σ . (D) Images of the sphere/plane contact in C for $P = 0.55 \text{ N}$. (D, Left) $Q = 0$. (D, Right) $Q = Q_s$. (Scale bars: 1 mm.)

$$Q_s = \frac{1}{2\alpha_R\sigma} \left(\sqrt{1 + 4\sigma^2\alpha_R A_0^R} - 1 \right). \quad [3]$$

Fig. 2B, Inset represents, for all experiments (various types of interfaces, normal loads, velocities, roughness), the value of Q_s estimated by Eq. 3 as a function of its measured value. All points align on the equality line, showing good accuracy and robustness of our estimate. How much is Eq. 3 improving the estimate of Q_s with respect to the uninformed estimate, σA_0^R , made when one ignores the dependence of A^R with Q ? To answer this, we plot in Fig. 2B (main plot) the relative difference between the two estimates as a function of the corresponding relative difference between A_s^R and A_0^R . Both differences are found roughly equal, showing that the observed area reductions, up to 30%, can lead to 30% overestimations (resp. underestimations) of Q_s (resp. σ) when the only available information about A^R is its initial value A_0^R .

This is practically important because most available models for the area of real contact in randomly rough contacts predict only A_0^R , as they consider interfaces under purely normal load (e.g., refs. 4, 13–16). A first-order improvement of these models would be to include the effect of incipient tangential loading and associated area reduction. They could then provide better estimates of the adhesive, purely interfacial, contribution to static friction quantified by σ . The viscoelastic, bulk contribution to friction would also be better estimated because the models would account for the reduced size of the microjunctions in the loading direction, which controls the excitation frequencies of the viscoelastic bodies.

A Common Behavior Across Scales

Now that our working hypothesis (in elastomers, the area of rough contacts, like that of smooth contacts, decreases with increasing shear) has been validated, we go farther and compare the reduction laws of A^R and A^A . To do this, we carried out additional experiments to measure A^A on smooth contacts between PDMS spheres of millimetric radius of curvature (*Materials and Methods*) and the same substrates previously used for rough contacts. Under increasing shear, those contacts start circular and

progressively become ellipse-like, as classically found (33–36) (Fig. 2D). As far as the contact area is concerned, for all interface types, sphere/plane contacts behave exactly as multicontacts (compare Fig. 2C and 2A). In particular, the area reduction law is also captured by a quadratic form $A^A(Q) = A_0^A - \alpha_A Q^2$, identical to Eq. 1, with α_A the reduction rate associated with the apparent area of individual contacts, as opposed to α_R related to the real area of multicontacts. The evolution of A_0^A with P is captured by the Johnson–Kendall–Roberts (JKR) model for adhesive sphere/plane contacts (43) (Fig. S3). The threshold law is again $Q_s = \sigma A_s^A$. The ingredients behind Eq. 3 being the same as for multicontacts, the estimate of Q_s for sphere/plane contacts is just as good (circles in Fig. 2B).

Such sphere/plane contacts are often considered good proxies for individual microjunctions in rough contacts. One advantage is that the tangential load can be measured directly for sphere/plane contacts, whereas it is inaccessible for an individual microjunction. This allows us to show, in Fig. 3 (circles), that for PDMS/glass sphere/plane contacts, α_A decreases with A_0^A as a power law with an exponent close to $-3/2$. We find it true for monocontacts of all types (Fig. S4).

To compare this behavior with that of individual microjunctions, we track, along each experiment, the area evolution of the individual microjunctions. Assuming they also obey a quadratic reduction law like Eq. 1, their individual α_{Ai} are estimated as (*Materials and Methods*) $\alpha_{Ai} = (A_{0i}^A - A_{si}^A)/(\sigma^2 A_{si}^A{}^2)$, with σ the shear strength of the macroscopic contact. The α_{Ai} are plotted as a function of A_{0i}^A in Fig. 3 (squares). Strikingly, the dependence of α_A on the initial area, A_0^A , appears identical (power law of exponent around $-3/2$) within experimental accuracy for microjunctions and sphere/plane contacts, over four orders of magnitude of A_0^A . We find it true for interfaces of all types (Fig. S4).

Behavior of Fingertip Contacts

To illustrate the generality of our results, analogous experiments were carried out on biological contacts between human fingertips and bare glass (Fig. 4 and *Materials and Methods*). Real contact occurs only along the protruding fingerprint ridges (Fig. 4C) (37, 38, 44, 45). The evolution of the area of real contact is shown in

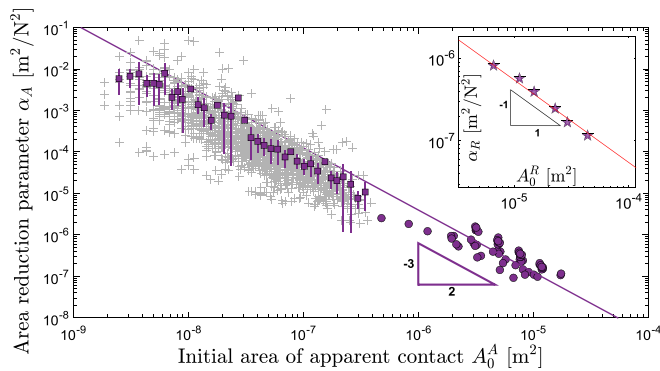


Fig. 3. Area reduction across scales: α_A vs. A_0^A (PDMS/glass interface). Circles: sphere/plane contacts for all R . $V = 0.1$ mm/s. +: raw data for microjunctions within multicontacts ($R_q = 26$ μ m). Squares: average of the positive raw data divided into 40 classes. Bars show SD within each class. Line: guide for eyes with slope $-3/2$. Inset: α_R vs. A_0^R for the same multicontacts. Inset line: guide for eyes with slope -1 .

Fig. 4A as a function of the tangential force applied, Q . Interestingly, A^R evolves under shear in a way very similar to that of elastomeric contacts (compare Fig. 4A with Fig. 2A and C). First, we find that a quadratic reduction law like Eq. 1 captures reasonably the data (although a linear fit would also be acceptable). Second, we find a linear threshold law like Eq. 2. As a consequence, Eq. 3 successfully predicts the value of the static friction force of fingertip contacts (blue diamonds in Fig. 2B).

As illustrated in Fig. 4B, we found that fingertip contacts under shear combine features of both sphere/plane contacts and planar multicontacts. As previously shown in the literature (37, 38), like sphere/plane contacts, their area of apparent contact (contours in Fig. 4C) decreases, by typically 40%. What we show here is that, simultaneously, the individual area of each microjunction also decreases, by about 10%. Both effects combine to give a reduction of about 45% of the area of real contact ($45\% \simeq 40\% + 10\%$ of the remaining 60%).

Discussion

We now discuss the possible physical origins of the reduction in area of real contact and the quantities controlling the value of the reduction parameter α_R . As mentioned in the Introduction, reduction of the area of apparent contact A^A under shear has already been observed on smooth sphere/plane elastomeric contacts (33, 35, 36). Because we showed that A^A and A^R actually follow analogous reduction behaviors (Fig. 2A and C), they may very well result from similar phenomena but at different scales. Two approaches have been proposed in the literature to interpret the observations on A^A .

The first approach focuses on the role of viscoelasticity, relating area reduction to the increase of elastic modulus of a viscoelastic body on which a rigid rough body is steadily sliding. This approach has been used both for smooth spherical (40, 46) and rough planar (14, 47) frictionless indentors and predicts a sliding-velocity-dependent amplitude of the area reduction. Note that in our experiments, α_A has a measurable, but weak velocity dependence. Loading-induced stiffening was also invoked to explain the apparent contact reduction in fingertip contacts (38). However, although in apparent agreement with our observations, the abovementioned viscoelastic models cannot explain them. The reason is that, in our experiments, the geometry is opposite: The rigid body is smooth and flat. Thus, in a steady sliding regime, the viscoelastic body (sphere or rough plane) experiences a deformation which is constant in time and thus is not affected by viscosity. In those conditions, the viscoelastic models would predict a recovery of the contact area to the value it had

before shearing, i.e., under purely normal load. This is in striking contrast to our sphere/plane experiments, in which both the area and the shape of the steady sliding apparent contact remain significantly modified with respect to the initial situation (Fig. 2D). Additional experiments, in which shear loading is interrupted before the onset of sliding, show that, contrary to what viscoelastic models would have predicted, the area does not come back to its initial value. Those qualitative discrepancies suggest that viscoelasticity is not responsible for our observations.

The second approach focuses on the role of adhesion and describes the motion of the contour of sphere/plane contacts as a crack propagating under mixed-mode loading (opening plus shear). Unfortunately, all existing theoretical models (33, 36, 39) treat the case of axisymmetric shrinking of the contact area, an assumption which is strongly violated in our experiments (Fig. 2D). We believe that those models can anyway help us identify the mechanisms involved in the shear-induced area reduction. The two most recent models (36, 39) consider that the area reduction results from a combination of peeling at the contact's periphery (points in contact are lifted up from the glass) and microslipping in an annular peripheral region of the contact. To assess whether those mechanisms are involved in our experiments, we gently scratched an elastomer sphere to introduce small defects within the contact image that could be tracked during shearing experiments. Those experiments showed that for sphere/plane contacts, the area reduction is indeed related to both predicted contributions: (i) peeling at the trailing edge of the contact, partially compensated by the opposite behavior at the leading edge, collectively responsible for typically half of the total reduction, and (ii) compression of the contact in the loading direction due to heterogeneous slip, responsible for the other half of the reduction.

Given the good qualitative agreement of the adhesion-based models with our experiments, it is worth looking more quantitatively into their behavior. We carried out a numerical analysis of the model of ref. 36 and found that the beginning of the predicted area reduction is well fitted by a quadratic decay with the tangential load, in agreement with our observations. Independent variations of all model parameters allowed us to extract the scaling

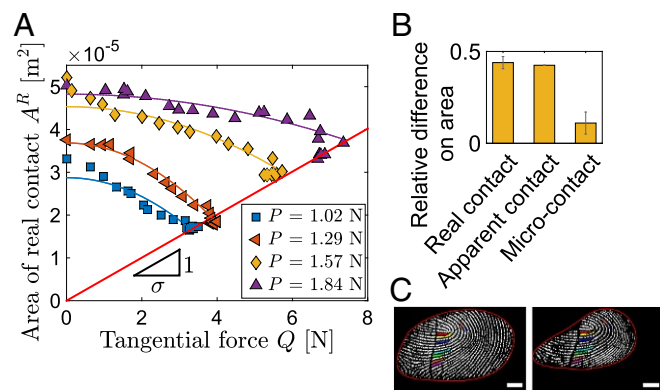


Fig. 4. Area reduction in human fingertip contacts. (A) A^R vs. Q , for various normal loads P (1 point of 190 shown). $V = 0.1$ mm/s. Curves: quadratic fits of the form of Eq. 1. Line: linear fit through the data corresponding to the onset of macroscopic sliding, passing through origin. See *Materials and Methods* for the value of σ . (B) Relative area difference between initial and final contact. B, left: area of real contact, A^R (error bar: segmentation threshold modified by ± 3 gray levels). B, center: area of apparent contact, A^A (error bar: same as B, left). B, right: individual area of 10 selected microjunctions (colored in C) that remain in contact all along the experiment (error bar: \pm SD). (C) Binarized image of a typical contact ($P = 1.57$ N). Red line: contour of the apparent area of contact. (Scale bar: 3 mm.) C, Left: $Q = 0$. C, Right: steady sliding.

relationship $\alpha_A \sim \frac{R^{0.18}}{E^{0.65} w_0^{0.47} P^{0.86}}$, with R the sphere's radius, E its Young's modulus, and w_0 the interface's work of adhesion. Interestingly, the exponent of the P dependence is close to -1 . Considering that, for elastic sphere/plane contacts, P scales as $(A_0^A)^{3/2}$, this exponent is in good agreement with the exponent $-3/2$ found for individual contacts in Fig. 3. Although R was changed threefold and w_0 twofold, those ranges are not sufficiently large to test the corresponding scalings. The quite large negative exponent associated with E suggests that α_A becomes smaller when the contacting bodies are stiffer. This could explain why the reduction of the area of apparent contact under shear has mainly been reported for soft materials, like rubber or human skin, but not for instance for polymethylmethacrylate or glass (5, 17). It also suggests that in stiff plastic materials like metals, the area reduction is likely much smaller than the concurrent plasticity-induced growth of the area, explaining why only the latter has been reported. Although the model of ref. 36 appears scaling-wise consistent with our results on smooth spherical contacts, there is currently no available adhesion-based model for area reduction in rough contacts to compare with our data.

Irrespective of the precise mechanisms involved in area reduction, the phenomenon has important fundamental implications. First, we observed that (i) the reduction of area of real contact in rough contacts is the macroscale consequence of the shrinking of the individual microjunctions (Fig. 1B, *Inset*) and (ii) the reduction parameter α_A of microjunctions obeys a well-defined scaling law of the form $\alpha_A = \beta(A_0^A)^{-\gamma}$. Those two observations suggest that macroscale reduction could be understood from that of the microjunctions, through a statistical average, along the lines of previous statistical friction models (13, 48). In *SI Notes, Mean-Field Model Relating α_A and α_R* , we indeed derive the expression of the macroscale reduction parameter, α_R , in terms of the parameters of the microscale scaling law, β and γ , in the simple case of a multicontact made of identical, independent microjunctions. The main outcome of this mean-field approach is that the scaling of α_R with the initial area A_0^R is different from that of α_A . Within the assumptions used, we find that $\alpha_R \sim (A_0^R)^{-1}$, independent of the microscopic exponent γ . As shown in Fig. 3, *Inset*, this scaling actually captures very well the observed dependence of α_R with A_0^R for our macroscopic, rough contacts. Thus, it is now possible, for elastomers, to incorporate the shear-induced variations of the area of real contact in multiscale friction models like refs. 48–54, through the microscopic law $\alpha_A = \beta(A_0^A)^{-\gamma}$.

In the Introduction, we also argued that the success of the rate-and-state friction (RSF) law was due to the fact that it incorporates the three main recognized dependencies of the area of real contact. To what extent is the fourth dependency identified here affecting the way we understand the RSF law? The Rice–Ruina formulation of the RSF law (18, 24–26) involves a parameter, B , which is also the prefactor of the logarithmic increase of the static friction coefficient with the time spent at rest by the interface. If one neglects structural aging, such an increase is caused by the growth, in the same proportion, of the area of real contact due to asperity creep at rest (geometrical aging). Our results indicate that, at least for elastomers and human skin, before the static friction threshold is reached, the already aged area will decrease as the shear loading is increased. Thus, the area relevant to the static friction coefficient will be smaller than that expected if geometric aging was the only mechanism involved. As a consequence, interpreting the parameter B as a quantifier of geometrical aging alone leads, for those soft materials, to a systematic underestimation of the rate of geometrical aging of an interface (shown in *SI Notes, Reinterpretation of the Parameter B in the RSF Law*). We suggest that B instead represents a combination of the classical geometrical aging and of the shear-induced area variations, an idea already proposed for rocks (28). Our results are thus expected to directly impact (for the class of

soft materials studied here) or inspire the many scientific fields in which friction and RSF in particular are useful, including tribology, earthquake/landslide science, and robot/human haptics.

Materials and Methods

Mechanical Aspects. Driving of the slider is obtained using a motorized translation actuator (Newport LTA-HL). The tangential force Q is measured using a stiff piezoelectric sensor (Kistler 9217A) placed close to the motor. The Q signals are digitized and recorded at a sampling rate of 3 kHz (1 kHz for sphere/plane contacts and fingertip contacts). The normal and tangential forces, P and Q , are measured with 0.1 mN and 1 mN accuracies, respectively. For planar rough contacts, the slider is driven through a horizontal steel wire of stiffness $9,700 \pm 200$ N/m. For sphere/plane contacts and fingertips, the slider is driven rigidly through the length of a cantilever beam of bending stiffness 52 ± 1 N/m. The elastomer blocks ($35 \times 20 \times 2$ mm³ in x,y,z for $R_q = 26$ μ m, $21 \times 19 \times 2$ mm³ for $R_q = 20$ μ m) are made of PDMS (Sylgard 184, mass ratio 10:1) degassed during 1 h and cross-linked at ambient temperature during about 150 h. Its Poisson ratio is $\nu = 0.5$ (incompressible material). Its Young's modulus is measured to be $E = 1.6 \pm 0.1$ MPa [value (error bar): mean (SD) over all experiments using different spheres on PDMS/glass interfaces]. The rough free surface of each elastomer block is obtained by molding the polymer against a roughened steel plate. The height distribution of the steel plate was characterized with a tactile profilometer (Surfscan Somicronic) and found to be Gaussian, with a rms roughness R_q of either 20 μ m or 26 μ m. The smooth spherical PDMS caps used for sphere/plane contacts were obtained by molding against optically smooth concave optical lenses of radius $R = 7.06$ mm, 9.42 mm, or 24.81 mm.

Substrate Preparation.

Bare glass plates. Bare glass plates are obtained from Mirit Glas. Before experiments, the surface is washed with soapy water, then with ethanol, and eventually with distilled water. This process is repeated three times.

Glass coated with grafted PDMS chains. Microscope glass slides are cleaned by immersion in piranha solution [70/30 (vol/vol) of concentrated H₂SO₄ and H₂O₂] for 30 min at 50 °C. The solution is decanted, and the slides are rinsed with deionized water. They are then dried under a stream of N₂ gas, exposed to UV/ozone (cleaning plasma) oxidation for 6 min immediately before the deposition of organosilicon, and finally rinsed with ultrapure water. The entire cleaning process provides activated microscope glass slides, with clean and oxidized surfaces containing mainly Si-OH groups. A 100-mg/mL PDMS solution (in HPLC toluene) is passed through a microfilter to remove impurities. A drop of this solution is deposited onto an activated glass slide, which it is then spin-coated at 2,000 rpm for 30 s. The film is cured at 130 °C for 4 h. The surface is then rinsed in toluene for 2 h and dried with N₂. The resulting surface is covered with PDMS chains grafted at one end on the glass, with grafting density low enough for the rest of the chain to adsorb on the surface.

Glass coated with cross-linked PDMS. A PDMS elastomer base/curing agent mixture (mass ratio 10:1) of Sylgard 184 is poured into a mold composed of two glass plates separated by a polytetrafluoroethylene spacer either 1 mm (sample in Fig. 1) or 150 μ m (sample in Figs. S2 and S4) thick. After cross-linking at room temperature for 150 h, one glass plate is peeled away, leaving the other with a smooth elastic coating to be used for friction experiments.

Interfacial Properties. The work of adhesion of each interface type involving PDMS was obtained by fitting $A_0^A(P)$ for sphere/plane contacts, using the JKR model (43). The data were obtained on a dedicated apparatus. We found $w_0(\text{PDMS/glass}) = 27 \pm 1$ mJ/m² (agrees with ref. 36), $w_0(\text{PDMS/grafted}) = 30 \pm 1$ mJ/m² (smaller than in ref. 12), and $w_0(\text{PDMS/cross-linked}) = 65 \pm 3$ mJ/m² (larger than in ref. 55). The shear strengths of the various interface types were obtained as in Fig. 2A. For multicontacts, $\sigma(\text{PDMS/glass}) = 0.23 \pm 0.02$ MPa (agrees with ref. 7), $\sigma(\text{PDMS/grafted}) = 0.14 \pm 0.02$ MPa, and $\sigma(\text{PDMS/cross-linked}) = 0.34 \pm 0.05$ MPa (coating thickness 1 mm). For sphere/plane contacts, $\sigma(\text{PDMS/glass}) = 0.36 \pm 0.01$ MPa (agrees with ref. 56), $\sigma(\text{PDMS/grafted}) = 0.07 \pm 0.01$ MPa (agrees with ref. 12), and $\sigma(\text{PDMS/cross-linked}) = 0.23 \pm 0.01$ MPa (larger than in ref. 9).

Image Analysis. Images are recorded using a CCD camera (Flare 2M360 MCL, 8 bits, 2,048 \times 1,088 square pixels) at 300 frames per second (100 frames per second for sphere/plane and fingertip contacts). The pixel size in multicontact images was typically 25 μ m. Possible implications of this finite pixel size on area measurements are discussed in *SI Notes, Possible Implications of the Finite Optical Resolution of the Images*. To select the threshold used to binarize images, we used a method fully justified in *SI Notes, Contact Area*

Measurement, and summarized here. We fitted the intensity histogram of each image by a sum of two subhistograms: (i) one for the class of out-of-contact pixels (large intensities), the shape of which (distorted Gaussian) was inspired by the histogram of images fully out of contact, and (ii) one for the class of in-contact pixels (Gaussian). The threshold was taken at the intersection between the two subhistograms, which minimizes the probability to select a wrong class during thresholding. Along one experiment, the calculated threshold remains stable within ± 2 gray levels. It is thus taken as constant for each experiment at its mean value. It is found to increase by about 10 gray levels as the normal load increases from 1 N to 6 N. Tracking was performed as in ref. 57. To estimate α_{Ai} of microjunctions (Fig. 3), individual values of A_{0i}^A and A_{fi}^A are the (nonquantified) initial and final values of the sigmoid fitted onto $A_i^A(t)$.

Fingertip Experiments. They were done similarly to those in ref. 45. The protocols were approved by the Board of Directors of the Laboratoire de Tribologie et Dynamique des Systèmes. The subject (one of the authors) gave his informed consent. The right forefinger (male, 24 y old, right-handed Caucasian) is pointing upward and constrained in a fixed position at about

30° from the surface (bare glass). The glass is pressed under constant normal load, in the range 1–2 N, and moved at constant speed $V = 0.1$ mm/s in the distal direction. Before each experiment, the fingertip is cleaned with ethanol using a nonwoven paper to limit dust contamination. The glass is cleaned the same as for PDMS/glass experiments. Each experiment starts after a waiting time of 1 min (time necessary for the contact size to stabilize). The shear strength of our fingertip/glass interfaces was measured to be $\sigma = 0.20 \pm 0.01$ MPa.

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Supporting Information

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SI Notes

Contact Area Measurement. In digital images of multicontact interfaces (e.g., Fig. 1B), real contact regions appear with low gray levels whereas out-of-contact regions correspond to higher gray levels. We can thus classify the pixels using a threshold on their gray level. The threshold value is determined automatically as explained in the following.

Maximum a posteriori thresholding. The idea is to formulate the thresholding as a two-class classification problem. A given pixel can belong to class C_1 of contact pixels or to class C_2 of out-of-contact pixels and we want to assign it the best class based on its gray level z . If we can build a conditional probabilistic model giving the probability of having one class given the gray level, the classification problem can be solved using the maximum a posteriori (MAP) decision rule.

Formally, we denote $p(C_1|z)$ (respectively $p(C_2|z)$) the probability for a pixel to be in class C_1 (respectively C_2) given its gray level z . The best class assignment \hat{k} is given by

$$\hat{k} = \arg \max_{k \in \{1,2\}} p(C_k|z), \quad [\text{S1}]$$

with $\arg \max$ the operator returning the argument of a function at its maximum.

In practice the posteriors $p(C_k|z)$ are not always available and Bayes' theorem is used to decompose them as

$$p(C_k|z) = \frac{p(C_k)p(z|C_k)}{p(z)}, \quad k \in \{1,2\}.$$

The evidence term $p(z)$ being independent from the classes, Eq. S1 can be written as

$$\hat{k} = \arg \max_{k \in \{1,2\}} p(C_k)p(z|C_k). \quad [\text{S2}]$$

If the two conditional densities $p(z|C_k)$ (likelihoods) are unimodal, there exists a unique threshold level \hat{z} such that

$$\begin{cases} p(C_1)p(z|C_1) < p(C_2)p(z|C_2) & \text{if } z < \hat{z} \\ p(C_1)p(z|C_1) \geq p(C_2)p(z|C_2) & \text{if } z \geq \hat{z} \end{cases}$$

This threshold \hat{z} is a solution of the equation

$$p(C_1)p(z|C_1) = p(C_2)p(z|C_2). \quad [\text{S3}]$$

Probabilistic model. To find the optimal threshold, we need to model the two terms of Eq. S3. These terms can be estimated from the image histogram, assuming a parametric model of the two classes C_1 and C_2 . Indeed, the normalized histogram $h(z)$ of gray levels of an image to be segmented is an estimation of the probability density function $p(z)$ of gray levels in this image. Given the two pixel classes, we have

$$h(z) = p(C_1)p(z|C_1) + p(C_2)p(z|C_2). \quad [\text{S4}]$$

In Fig. S5C, we note the two modes of the histogram corresponding to the two terms of Eq. S4.

Parametric model. We choose to model each of the two classes by a parametric model inspired by the shape of the corresponding histograms. For the contact class, a Gaussian distribution is assumed,

$$G_{\mu,\sigma}(z) = \frac{1}{\sigma\sqrt{2\pi}} \exp\left(-\frac{(z-\mu)^2}{2\sigma^2}\right), \quad [\text{S5}]$$

with σ the SD of the Gaussian and μ its mean. Note that σ may include second-order nonlinear effects of light transmission through air where the two solids are separated by a gap smaller than the light's wavelength.

For the noncontact class, an empirical distribution (distorted Gaussian) was inspired by the histogram of the images completely out of contact (Fig. S5D). Its form is given in Eq. S6,

$$F_{b,c,d}(z) = a \exp\left(\frac{z-b}{c}\right)^2 \log(1 + \exp 0.1(z-d)), \quad [\text{S6}]$$

with a a normalization parameter, c a parameter related to the SD of the distribution, b a parameter related to its mean, and d an adjustable parameter.

The histogram can then be written as

$$h(z) = \Pi_1 G_{\mu,\sigma}(z) + \Pi_2 F_{b,c,d}(z), \quad [\text{S7}]$$

with $p(C_1) = \Pi_1$, $p(C_2) = \Pi_2$, $p(z|C_1) = G_{\mu,\sigma}(z)$, and $p(z|C_2) = F_{b,c,d}(z)$.

Parameter estimation. Knowing the histogram of an image to be segmented, we can determine priors Π_1 and Π_2 and the parameters of the distributions by a least-squares fitting from Eq. S7. Once the parameters have been identified, the segmentation can be defined from the threshold obtained at the intersection of the two functions representing each term of Eq. S7.

Threshold. The position of the intersection is given immediately as an output of the adjustment process, with an accuracy of ± 3 gray levels (green line in Fig. S5C). Along an experiment, i.e., considering all the images one by one, we found that the threshold calculated this way remains stable within ± 2 levels of gray. Given this stability, we have chosen to use a fixed threshold for all images of the same experiment. This threshold is obtained as an average over all individual thresholds along the experiment. It is found to increase by about 10 gray levels as the normal load increases from 1 N to 6 N.

Fig. S5 E and F shows the results of the segmentation of images in Fig. S5 A and B, respectively, using the above-described method. White spots correspond to microjunctions. The great resemblance between the black spots of the image in Fig. S5A and the white spots in Fig. S5E, together with the quasi-absence of white spots in Fig. S5F, validates the adopted segmentation method. More quantitatively, if the image in Fig. S5A is segmented using the extremal values of the likelihood interval of the threshold over time (typically $X \pm 3.5$ with X around 50), we find that the relative variation on the contact area is lower than 7.7% between min and max.

Mean-Field Model Relating α_A and α_R . Greenwood and Williamson's model (13) describes a rough surface as a collection of independent spherical asperities, all with the same radius of curvature R and with a random height distribution with SD s . In the case of an exponential distribution, Baumberger and Caroli (18) observed that the average area of a microjunction is $A_0^{A,m} = \pi R s$, independent on the normal load. As a consequence, the number of microjunctions involved in the multicontact grows linearly with the total area of real contact.

Based on these observations, we consider a mean-field model in which multicontacts are made of N identical, independent microjunctions of individual initial area $A_0^{A,m}$, such that the initial macroscopic area of real contact is $A_0^R = N A_0^{A,m}$. Based on the results of Fig. 2C, we further assume that, when the interface is sheared with a tangential force Q , each microjunction obeys a quadratic area reduction law of the form

$\overline{A^{A,m}} = \overline{A_0^{A,m}} - \alpha_A q^2$, with $q = Q/N$ and α_A the tangential load applied on and the area reduction parameter of each individual microjunction, respectively. Finally, based on the scaling law in Fig. 3, we also assume that $\alpha_A = \beta A_0^{A,m^\gamma}$.

The macroscopic area reduction law will then be obtained by rewriting the expression $A^R = N \overline{A^{A,m}}$,

$$A^R = N \left(\overline{A_0^{A,m}} - \beta \overline{A_0^{A,m}^\gamma} q^2 \right) \quad [\text{S8}]$$

$$= N \overline{A_0^{A,m}} - N \beta \overline{A_0^{A,m}^\gamma} \frac{Q^2}{N^2} \quad [\text{S9}]$$

$$= A_0^R - \beta \frac{\overline{A_0^{A,m}^\gamma}}{N} Q^2 \quad [\text{S10}]$$

$$= A_0^R - \beta \frac{\overline{A_0^{A,m}^{\gamma+1}}}{A_0^R} Q^2, \quad [\text{S11}]$$

meaning that $\alpha_R = \beta_R (A_0^R)^{-1}$, with $\beta_R = \beta \overline{A_0^{A,m}^{\gamma+1}}$ being a constant independent of A_0^R (and of P). The obtained scaling ($\alpha_R \sim (A_0^R)^{-1}$) is in good agreement with the data shown in Fig. 3, *Inset*.

Reinterpretation of the Parameter B in the RSF Law. The Rice and Ruina formulation of the RSF law (23) is usually given as (18, 25, 26)

$$\mu(V, \theta) = \mu_0 + A \ln \left(\frac{V}{V_0} \right) + B \ln \left(\frac{V_0 \theta}{D_c} \right), \quad [\text{S12}]$$

$$\dot{\theta} = 1 - \frac{V \theta}{D_c}, \quad [\text{S13}]$$

with V the sliding velocity, V_0 an arbitrary reference velocity, D_c a critical slip length, and θ a state variable.

In the static case ($V = 0$), $\theta = t$, so for long hold times we have

$$\frac{d\mu_s}{d(\ln(t))} = B, \quad [\text{S14}]$$

with $\mu_s = \frac{Q_s}{P} = \frac{\sigma A_s^R}{P}$ the static friction coefficient.

If one assumes that geometrical aging is the only mechanism involved in the selection of the area of real contact, Eq. S14 could be integrated as

$$A_{s,aging}^R(t) = A_0^R + \frac{PB_{aging}}{\sigma} \ln(t). \quad [\text{S15}]$$

Let us instead assume that after aging until time t , shear loading starts to be applied. The area of real contact of the aged interface, given by Eq. S15, corresponds to the initial area for the shear-induced reduction phenomenon. Assuming that shear loading is so fast that the additional geometrical aging is negligible during the time interval required to shear the interface from rest to the onset of sliding, Eq. 3 can be rewritten as

$$Q_s = \frac{1}{2\alpha_R \sigma} \left[\sqrt{1 + 4\alpha_R \sigma^2 \left(A_0^R + \frac{PB_{aging}}{\sigma} \ln(t) \right)} - 1 \right]. \quad [\text{S16}]$$

Using Eq. S14, the parameter B can now be evaluated from the derivative of Q_s with respect to $\ln(t)$, which gives

$$B = \frac{1}{P} \frac{dQ_s}{d(\ln(t))} = \frac{B_{aging}}{\sqrt{1 + 4\alpha_R \sigma^2 \left(A_0^R + \frac{PB_{aging}}{\sigma} \ln(t) \right)}}. \quad [\text{S17}]$$

Noting that $\sqrt{1 + 4\alpha_R \sigma^2 \left(A_0^R + \frac{PB_{aging}}{\sigma} \ln(t) \right)} = 1 + 2\alpha_R \sigma^2 A_s^R$ (replace Q_s with σA_s^R in Eq. S16 and reorganize), we can rewrite Eq. S17 as

$$B = \frac{B_{aging}}{1 + 2\alpha_R \sigma^2 A_s^R}. \quad [\text{S18}]$$

Eq. S18 directly shows that, due to shear-induced area reduction, B is always smaller than the value that one would expect (B_{aging}) if geometrical aging was the only mechanism at play. In other words, interpreting B as a direct quantifier of geometrical aging alone amounts to underestimating the rate of aging at the interface. To get a better sense of how much the underestimation is, remember that $\alpha_R \sigma^2 A_s^R$ corresponds to the relative area reduction due to shear (*Onset of Sliding* in main text). We have observed relative area reductions up to about 30%, so that the denominator of Eq. S18 can be up to about 1.6, meaning that the rate of aging may be underestimated by up to about 40%.

Possible Implications of the Finite Optical Resolution of the Images.

The optical resolution of any digital image is limited to the pixel lateral size s , typically 25 μm in our multicontact images. As a consequence, any structure of the area of real contact with a length-scale smaller than s cannot be resolved. This limitation may affect our measurements of A^R in two ways.

First, patches of real contact may contain holes that are out of contact and smaller than s^2 . This effect would lead to an overestimation of A^R . To assess whether this case is frequent, we considered typical microjunctions and imaged them with different zoom magnitudes (see Fig. S6 for a typical example). When reducing the pixel size by a factor of 3 (maximum zoom available with our optical device), i.e., by reducing the pixel area by about one order of magnitude, we uncovered very few holes, so that the area measurement of microjunctions was virtually unaffected by the change of resolution. The fact that only few holes can be observed is qualitatively consistent with the low Young's modulus of PDMS which, under the action of adhesive stress, will easily deform to conform to the rigid substrate.

The second effect is that microjunctions with an area smaller than $A_{pix} = s^2$ have a low probability to be detected, leading to an underestimation of A^R . To quantify the missing area due to this effect, we characterized the probability density function (pdf) of the areas of individual microjunctions in unsheared interfaces, A_{0i}^A . We found that, for all normal loads, those pdfs are reasonably fitted by power laws, i.e., with a form $p(A_{0i}^A) = K(A_{0i}^A)^{-n}$. Assuming that this form is valid at all scales between 0 and the maximum microjunction size, $A_{0i,max}^A$, we can assess what the fraction is of the area that is constituted by microjunctions smaller than A_{pix} . The total area is given by

$$A_0^R = \int_0^{A_{0i,max}^A} A_{0i}^A p(A_{0i}^A) dA_{0i}^A = K \frac{(A_{0i,max}^A)^{2-n}}{2-n}, \quad [\text{S19}]$$

while the area missed due to the finite size of the pixels is

$$A_{0,missed}^R = \int_0^{A_{pix}} A_{0i}^A p(A_{0i}^A) dA_{0i}^A = K \frac{(A_{pix})^{2-n}}{2-n}. \quad [\text{S20}]$$

Finally, the fraction of missed area is $\frac{A_{0,missed}^R}{A_0^R} = \frac{(A_{pix})^{2-n}}{(A_{0i,max}^A)^{2-n}}$.

With n found close to 1.5 and $A_{0i,max}^A$ being larger than 100 A_{pix} , we estimate that $\frac{A_{0,missed}^R}{A_0^R} \simeq \sqrt{\frac{A_{pix}}{A_{0i,max}^A}} < \frac{1}{10}$. This means that, in our experiments, the fraction of the area constituted by microjunctions smaller than the pixel size is always smaller than 10%

and is usually smaller than 5%. This fraction is of the order of or smaller than that associated to the uncertainty on A^R due to the determination of the segmentation threshold. Note that such an error is an absolute error and can affect the measured value of σ ,

by the same fraction. In contrast, the evolution of the area under shear relative to the initial area is essentially unaffected by this absolute error and thus does not affect the main conclusions of the present study.

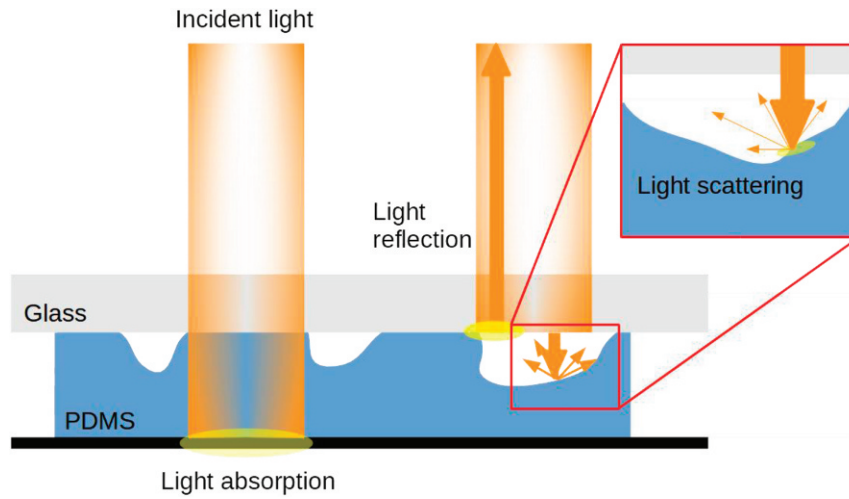


Fig. S1. Sketch of the light behavior at the interface. A rough PDMS sample (blue) in contact with a smooth glass plate (gray) is illuminated from the top by a diffuse white light. The light rays can be either transmitted through the real contact regions and absorbed by a black layer (bottom) or partly reflected by the glass/air dioptré and partly back scattered by the air/PDMS dioptré in out-of-contact regions.

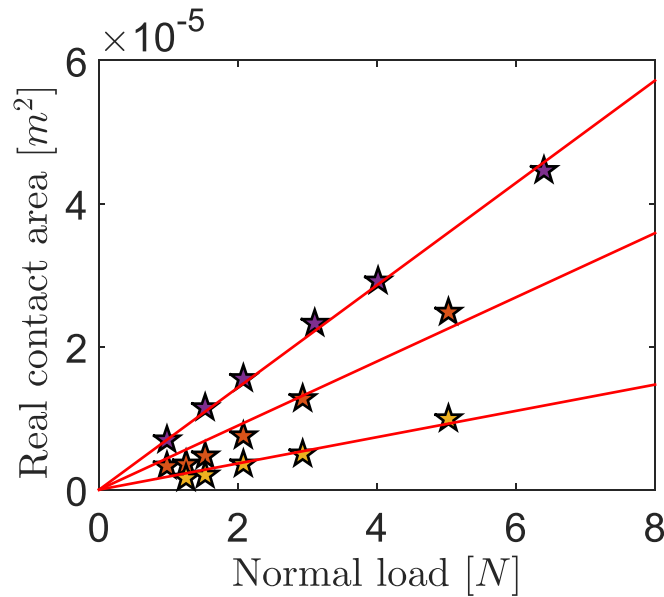
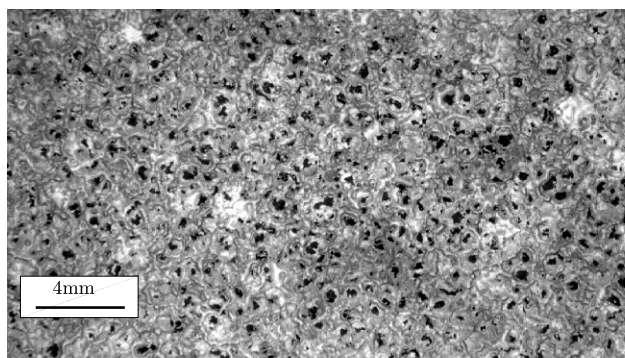
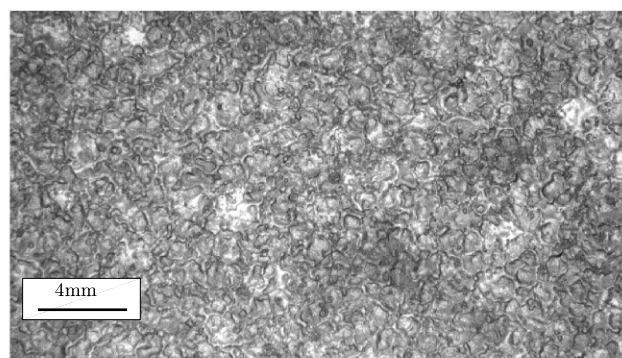


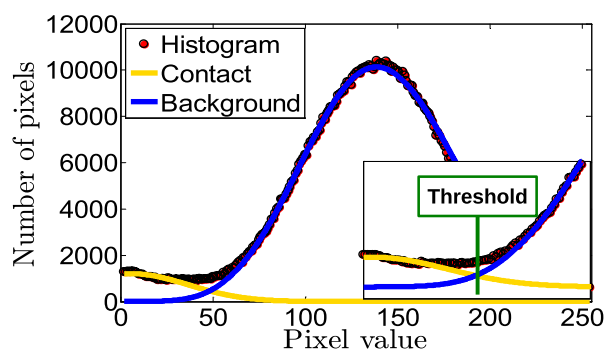
Fig. S2. Initial area of real contact is proportional to the normal load for multicontacts. Real contact area (for $Q=0$) as a function of the normal load is shown. Purple: PDMS/glass multicontacts ($R_q = 26 \mu\text{m}$). Orange: PDMS/cross-linked PDMS multicontacts ($R_q = 20 \mu\text{m}$). Yellow: PDMS/grafted PDMS multicontacts ($R_q = 20 \mu\text{m}$). Red lines: linear fits passing through the origin.



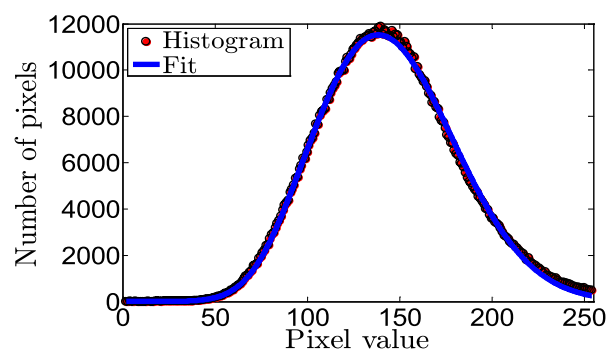
A



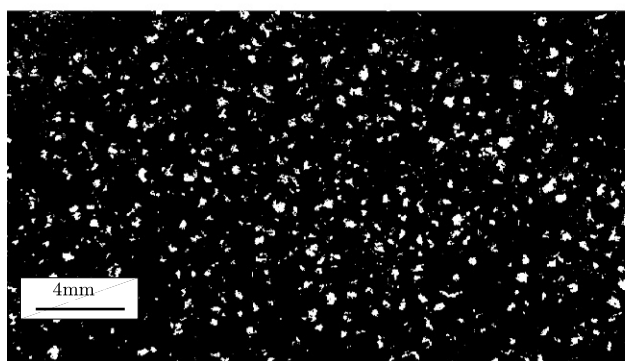
B



C



D



E



F

Fig. S5. Principle of the image segmentation. Shown is an example of a PDMS/glass multicontact, with $R_q = 26 \mu\text{m}$. (A) Raw contact image. (B) Raw non-contact image serving as a calibration for the shape of the out-of-contact histogram distribution. (C) Contact image histogram. (D) Out-of-contact image histogram. (E) Binarized contact image. (F) Binarized out-of-contact image.

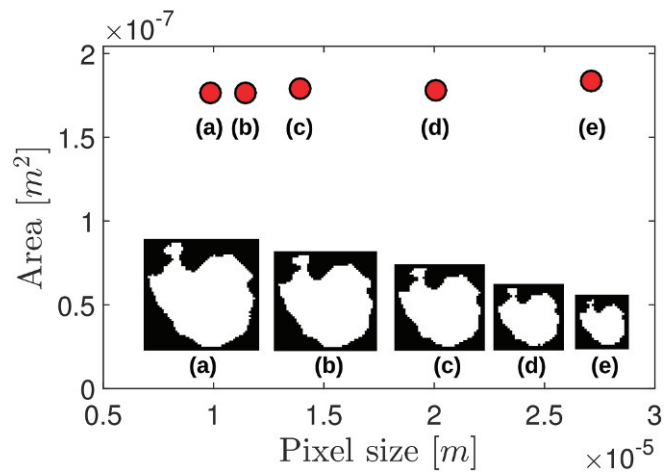


Fig. 56. Area measurements are essentially scale independent. Main plot (red circles) shows measured area of a microjunction as a function of the pixel size. Insets a–e show a segmented image of the same microjunction for various zoom-ins.